

# Fluorescence Biosensor for Real-Time Interaction Dynamics of Host Proteins with HIV-1 Capsid Tubes

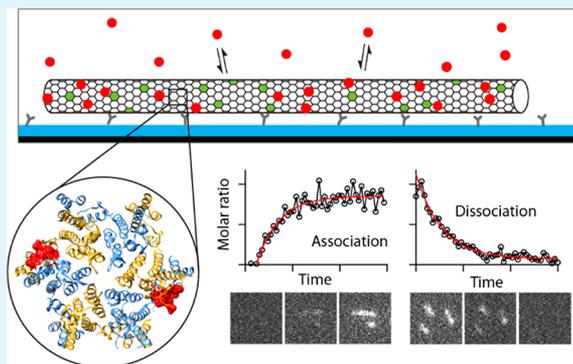
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## Supporting Information

**ABSTRACT:** The human immunodeficiency virus 1 (HIV-1) capsid serves as a binding platform for proteins and small molecules from the host cell that regulate various steps in the virus life cycle. However, there are currently no quantitative methods that use assembled capsid lattices to measure host–pathogen interaction dynamics. Here we developed a single-molecule fluorescence biosensor using self-assembled capsid tubes as biorecognition elements and imaged capsid binders using total internal reflection fluorescence microscopy in a microfluidic setup. The method is highly sensitive in its ability to observe and quantify binding, to obtain dissociation constants, and to extract kinetics with an extended application of using more complex analytes that can accelerate characterization of novel capsid binders.

**KEYWORDS:** HIV capsid, TIRF, binding, stoichiometry, kinetics, microfluidics



## INTRODUCTION

HIV-1 establishes infection by integrating its genome into a host chromosome. In order to access the DNA of the target cell, the viral genome must travel across the cytoplasm and enter the nucleus, while avoiding recognition and degradation by the host.<sup>1</sup> The vehicle responsible for conveying and protecting the genome on this journey is the HIV-1 capsid, a metastable nanocontainer comprising ~1500 copies of the capsid protein (CA) that assembles into a lattice of hexamers and pentamers to form a fullerene cone. While the capsid physically excludes host macromolecules from accessing the viral genome, its functions are more nuanced than a simple inert protective shell. In addition to avoiding cell autonomous immune responses, the capsid has roles in cytoplasmic trafficking,<sup>2</sup> reverse transcription,<sup>3</sup> nuclear entry, and integration site selection.<sup>4</sup> It must also release the viral genome prior to integration in an enigmatic process called “uncoating” (see the review in ref 5).

While the CA lattice persists within the target cell, the capsid represents the dominant host–pathogen interface. In this role, the lattice represents a binding platform for the recruitment of numerous host-derived molecules that the virus hijacks to mediate the above processes. Three binding sites on CA have been characterized largely using structural approaches, and each shows affinity toward at least two host cofactors. These sites are (1) the CypA-binding loop, comprising residues 85–93 which form a flexible structure on the capsid exterior responsible for recruiting cyclophilin A (CypA)<sup>6,7</sup> and the nucleoporin Nup358;<sup>8</sup> (2) the FG-binding site, a pocket on

the N-terminal domain of CA that binds to phenylalanine-glycine motifs of cleavage and polyadenylation specificity factor subunit 6 (CPSF6)<sup>9,10</sup> and a second nucleoporin, Nup153;<sup>10</sup> and (3) the central arginine pore formed by a cluster of five or six symmetry-related copies of Arg18 that recruit deoxyribonucleotides (dNTPs) and inositol hexakisphosphate (IP6).<sup>11,12</sup> The CypA-binding loop and FG-binding site are both believed to play roles in nuclear import and evasion of immune recognition. The central arginine pore, on the other hand, is believed to play roles in selective import of dNTPs for reverse transcription and in mediating capsid stability through recruitment of polyanions such as IP6. Importantly, the FG-binding site and the arginine pore are only formed in the assembled CA lattice, as they contain structural elements that are contributed by multiple adjacent CA monomers. In order to study capsid-binding compounds, it is therefore necessary to use a system that recapitulates the assembled CA lattice.

Current capsid binding assays are usually based on pull-down experiments using capsid as bait from either isolated cores,<sup>13–15</sup> in vitro assembled CA-NC tubes,<sup>16,17</sup> or disulfide cross-linked CA A14C/E45C tubes.<sup>18</sup> Quantitative methods such as isothermal titration calorimetry and surface plasmon resonance are possible using in vitro assembled soluble CA A14C/E45C/W184A/M185A hexamers,<sup>19,20</sup> but these methods are sample-intensive and not all CA interfaces (that would

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otherwise be present in fully assembled CA lattice for cofactor binding) are represented in the soluble hexamer.

Here we propose to overcome the limitations of existing methods with the design of an interface for capsid binders that has the sensitivity to visualize and quantify binding events at the single-molecule level using total internal reflection fluorescence microscopy (TIRFM). The biorecognition element consists of cross-linked and fluorescent CA tubes that are grown on the sensor surface inside a microfluidic device. The biosensor allows accurate measurements of interaction kinetics, affinity, and stoichiometry and is compatible with both purified recombinant CA binders and complex samples, such as cell-free expression lysates, enabling characterization of binders that might otherwise be difficult to isolate.

## MATERIALS AND METHODS

**Production and Labeling of Recombinant Proteins.** HIV-1 CA (wild-type, CA A14C/E45C and CA K158C) was expressed in bacteria and purified as previously described.<sup>21</sup> CA K158C was labeled as described.<sup>22</sup> CypA was expressed in bacteria, purified, and labeled as described.<sup>22</sup> Detailed methods for protein purification and labeling are available in the [Supporting Information \(SI\)](#).

**Fluorescence Labeling of CPSF6<sub>313–327</sub>.** A synthetic peptide from CPSF6 comprising residues 313–327 with a C-terminal cysteine (PVLFPGQPFPGQPPLGC, Genscript) was dissolved (1.85 mM) in 50 mM Tris buffer (pH 8) and reacted with Alexa Fluor 488-C5-maleimide (1.85 mM) for 10 min. Thin-layer chromatography (silica gel, methanol:water, 1:1, v/v) showed near quantitative incorporation of the fluorescent dye. CPSF6<sub>313–327</sub>-AF488 was flash frozen and stored at  $-40\text{ }^{\circ}\text{C}$ . The peptide was diluted to 50  $\mu\text{M}$  with buffer (50 mM Tris, pH 8, 1 mM DTT) prior to use.

**Negative Staining Electron Microscopy.** CA assembly mixture (1 M NaCl, overnight,  $4\text{ }^{\circ}\text{C}$ ) was applied to a 200 mesh Cu grid coated with carbon and Formvar (Ted Pella) and wicked dry. The sample was stained with a drop of uranyl acetate (2% w/v) and wicked dry immediately. This staining process was repeated three times and the grid was air-dried. Micrographs were collected using a FEI Tecnai G2 20. Tubes diameters were measured using ImageJ.

**Fabrication of Microfluidic Devices.** An aluminum lithography mold was used to cast polydimethylsiloxane microfluidic devices with five parallel flow channels ( $1000 \times 800 \times 60\ \mu\text{m}$ ,  $L \times W \times H$ ). The PDMS devices were treated with air plasma (3 min) and annealed to clean glass coverslips.

**Sensor Surface Modification and in Situ Assembly of CA Tubes.** Flow channels were incubated with a solution of PLL(20)-g[3.5]-PEG(2)/PEG(3.4)-biotin(20%) (1 mg/mL, SuSos AG) for 30 min. The channels were washed with water and incubated with streptavidin (0.2 mg/mL) in blocking buffer [20 mM Tris (pH 7.5), 0.4 mM EDTA, 50 mM NaCl, 0.006%  $\text{NaN}_3$ , 0.025% Tween 20, 0.2 mg/mL BSA] for at least 20 min. Tubing was inserted into the channel ports and the outlet tubing was connected to a syringe pump operated in withdraw mode at a flow rate of 30  $\mu\text{L}/\text{min}$ . Channels were rinsed with 50  $\mu\text{L}$  wash buffer [50 mM Tris (pH 8), 150 mM NaCl], filled with a solution (20  $\mu\text{L}$ , 1:3000 dilution) of biotinylated  $\alpha$ -mouse antibody (Jackson ImmunoResearch, 115-066-071) and  $\alpha$ -CA antibody (Advanced Biotechnologies, 13-102-100), and again rinsed with wash buffer (50  $\mu\text{L}$ ). To grow CA tubes on the sensor surface, a buffer solution [50 mM Tris (pH 8.0), 2 mM DTT, 0.02%  $\text{NaN}_3$ ] containing CA A14C/E45C (76  $\mu\text{M}$ ) and labeled CA K158C (AF488 or AF647, 4  $\mu\text{M}$ ) was mixed with high salt buffer [50 mM Tris (pH 8.0), 5 M NaCl] to give a final NaCl concentration of 500 mM, immediately injected into the flow cell, and incubated for 30 min. CypA (10  $\mu\text{M}$ ) was added to the assembly mixture to reduce tube bundling. The flow channel was then rinsed with wash buffer (50  $\mu\text{L}$ ). Before injection of analyte, the flow channel was rinsed with 100  $\mu\text{L}$  of imaging buffer [50 mM Tris (pH 8), 150 mM NaCl, 2 mM

Trolox, 2.5 mM protocatechuic acid, 0.25 U/mL protocatechuate-3,4-dioxygenase].

**Total Internal Reflection Fluorescence (TIRF) Microscopy and Image Analysis.** TIRF images were acquired (typical exposure time 10 ms) using an inverted microscope equipped with a Nikon 100 $\times$  CFI Apochromat TIRF oil immersion objective (1.49 NA), a NicoLase laser system,<sup>23</sup> and two Andor iXon 888 EMCCD cameras. Images were analyzed using home-written image analysis software for detection of tubes and extraction of binding/dissociation traces (<https://github.com/lilbutsa/JIM-Immobilized-Microscopy-Suite>). Fluorescence intensities in each region of interest were converted to the number of molecules using the intensity of a single fluorophore (determined by photobleaching) as a calibration factor.

**Equilibrium Binding Analysis To Determine  $K_d$  and Stoichiometry of CypA Binding to CA Tubes.** CypA solutions (1–40  $\mu\text{M}$ ) were prepared with CypA-AF647 (1  $\mu\text{M}$ ) and unlabeled CypA (added to make up the desired final concentration) in imaging buffer. The CypA solution (30  $\mu\text{L}$ ) was drawn into the channel (100  $\mu\text{L}/\text{min}$ ) and incubated for 1 min. TIRF images were recorded in several fields of view (FOV) in both channels using sequential excitation to measure the signals associated with CA tubes (491 nm) and colocalized CypA (639 nm). Subsequently, the CypA solution was washed out with imaging buffer (100  $\mu\text{L}$ ). Images were analyzed to determine the CypA:CA molar ratio reached at equilibrium for each CypA concentration. Binding curves were obtained by plotting the best fit molar binding ratio as a function of CypA concentration. The following equation was used for model fitting to obtain estimates for the dissociation constant and the maximum binding ratio,  $R(\text{eq}) = [\text{CypA}] \times R(\text{max}) / ([\text{CypA}] + K_d)$ , where  $R(\text{eq})$  is the CypA:CA ratio at equilibrium for a given CypA concentration,  $[\text{CypA}]$  is the concentration of CypA,  $R(\text{max})$  is the CypA:CA molar ratio at saturation, and  $K_d$  is the dissociation constant.

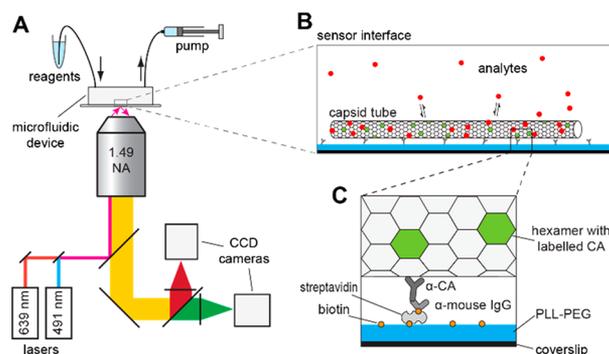
**Kinetics Analysis of CPSF6<sub>313–327</sub> Binding to CA Tubes.** Imaging buffer containing the analyte (CPSF6<sub>313–327</sub>-AF488, 250 nM) and a free dye as a marker for solution exchange in the flow channel (Alexa Fluor 647, 200 nM) was injected into the flow channel (100  $\mu\text{L}/\text{min}$ ) and subsequently washed out with imaging buffer (100  $\mu\text{L}/\text{min}$ ) while recording the CA K158C-AF647 and CPSF6<sub>313–327</sub>-AF488 channels by time-lapse TIRF imaging with a frame rate  $1/3\ \text{s}^{-1}$  (150 s for washin and 300 s for washout).

**Competition Binding of CPSF6 Peptide with PF74.** CPSF6<sub>313–327</sub>-AF488 (250 nM) in imaging buffer containing 2% DMSO or 10  $\mu\text{M}$  PF74 (from 0.5 mM stock in DMSO) was injected into the microfluidic flow cell (50  $\mu\text{L}$ , 50  $\mu\text{L}/\text{min}$ ), and TIRF images were recorded 5 min postinjection in five or more fields of view in both channels using simultaneous acquisition to measure CPSF6<sub>313–327</sub>-AF488 signals colocalizing with CA tubes (647 nm). CPSF6<sub>313–327</sub>-AF488 was subsequently washed out with 250  $\mu\text{L}$  of imaging buffer (50  $\mu\text{L}/\text{min}$ ) and the flow channel was reused for subsequent injections. Data were obtained from six independent injections from two different microfluidic flow channels.

**Biosensor Assay of Capsid-Binding Proteins Produced by Cell-Free Expression.** The open reading frame for CPSF6 (isoform 2) was cloned into a vector for cell free expression of the protein with His<sub>6</sub>-GFP fused to its N-terminus. In vitro expression of proteins was initiated by adding plasmid (60 nM) to *Leishmania* extract<sup>24</sup> supplemented with RNase OUT (Invitrogen), and the mixture was incubated in the dark at  $28\text{ }^{\circ}\text{C}$  for 2.5 h. Protein concentrations were estimated using single-molecule spectroscopy with recombinant eGFP as a standard.<sup>25</sup> The cell-free expression mixture was diluted with wash buffer (supplemented with 2 mM Trolox, 2.5 mM protocatechuic acid, and 0.25 U/mL protocatechuate-3,4-dioxygenase) to a final concentration of 370 nM GFP-tagged protein. This solution (40  $\mu\text{L}$ ) was drawn into the flow channel (100  $\mu\text{L}/\text{min}$ ) and subsequently washed out with imaging buffer (500 at 100  $\mu\text{L}/\text{min}$ ) while recording the CA K158C-AF647 channel and the GFP channel by time-lapse TIRF imaging.

## RESULTS AND DISCUSSION

**Biosensor Design.** The design of the total internal reflection fluorescence (TIRF) imaging-based sensor for measuring the interactions between HIV-1 capsid-binding molecules and self-assembled CA lattices in real time is shown in Figure 1. The sensor interface is assembled on the surface of



**Figure 1.** Schematic of the interface design. (A) The setup consists of a TIRF microscope for real-time observation of binding events on the sensor surface assembled on a glass coverslip located at the bottom of a PDMS microfluidic device for analyte delivery. (B) Fluorescent tubes self-assembled from HIV-1 CA serve as the receptor for capsid-binding analytes. Binding and dissociation of analytes is detected by the appearance and disappearance of the analyte signal colocalized with each individual tube. (C) The sensor surface is modified with an antifouling layer and antibodies for immobilization of fluorescent CA tubes.

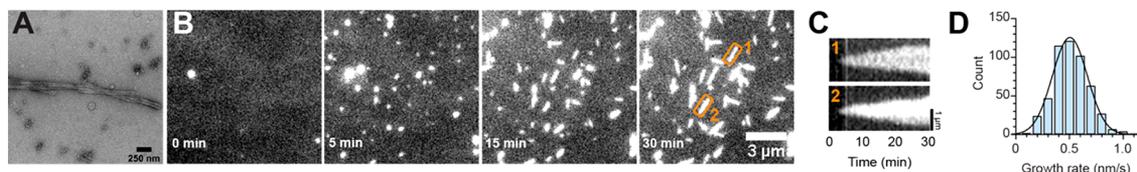
a glass coverslip that forms the bottom of a microfluidic channel device fabricated by soft lithography in PDMS. Cross-linked and fluorescent CA hexamer tubes are then self-assembled in situ and function as the biorecognition elements of the sensor. An analyte solution containing a (putative) capsid-binding species labeled with a different fluorescent dye is flowed through the channel while dual-color fluorescence movies are recorded using a TIRF microscope equipped with CCD cameras, whereby binding (or dissociation) of analytes can be visualized on individual tubes from the appearance (or disappearance) of fluorescence in the analyte channel. We then use single-molecule analysis of the fluorescence movies to extract kinetic parameters of the interaction. In the following, we first present the development of the sensor interface followed by applications of the sensor to measure binding affinity, stoichiometry, and kinetics of host proteins known to interact with the HIV-1 capsid to promote infection.

**Growth of Fluorescent Capsid Tubes on the Sensor Surface as Biorecognition Elements.** We used self-assembly of recombinant CA A14C/E45C at high salt concentrations to produce tubular lattices of disulfide cross-

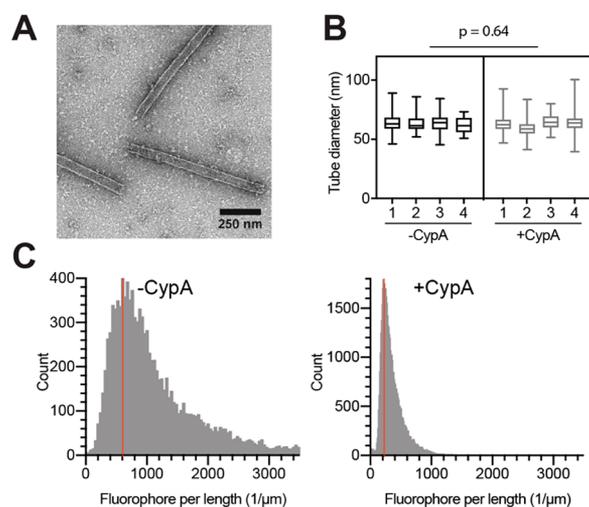
linked CA hexamers<sup>26</sup> as biorecognition elements representing the HIV-1 capsid.<sup>18</sup> These stabilized tubes were rendered fluorescent by coassembly with a small fraction of CA K158C reacted with a fluorophore at the engineered cysteine (Figures S1 and S2, SI). This coassembly reaction also yielded long tubes that aggregated into bundles in solution (Figure 2A), a process known to be driven by interactions between hydrophobic residues (primarily located in the CypA loop of CA) on the outer tube surfaces.<sup>27</sup> Initial attempts to deposit preassembled CA tubes onto surfaces failed, presumably because of excessive aggregation into large clusters.

Next, we investigated methods to grow tubes directly on the biosensor surface. The glass surface was first passivated by physisorption of a copolymer of poly(L-lysine) and biotinylated poly(ethylene glycol) (PLL-PEG-biotin) to resist nonspecific adsorption of biomolecules from solution (Figure 1C). The PLL-PEG-biotin surface was further modified with streptavidin followed by a biotinylated secondary antibody [anti-mouse IgG F(ab')<sub>2</sub> fragment] for capture of a primary mouse antibody directed against the exterior surface of CA.<sup>28</sup> Injection of an assembly mixture containing CA A14C/E45C and labeled CA K158C into the flow channel followed by incubation (30 min) resulted in the growth of capsid tubes on the modified surface, which appeared as fluorescent lines in the TIRF image (Figure S3, SI), which could easily be distinguished from the background on the basis of shape and intensity. Fluorescent lines were not observed on surfaces without antibodies (Figure S3A, SI), indicating that tube capture was specific. Time-lapse imaging of the assembly reaction on antibody-modified surfaces revealed the tube growth process (Figure 2B). Capsid seeds (presumably small CA assemblies formed in solution) were captured by the antibodies onto the surface, where they appeared as bright fluorescent puncta within 5 min of injecting CA assembly solution into the flow channel. Over the next 20 min these seeds grew bidirectionally by addition of CA from solution to the ends of the lattice into  $\sim 1 \mu\text{m}$  long tubes, consistent with previous observations.<sup>28</sup> The growth kinetics could be determined at the level of single tubes from kymographs generated along the tube axis, as shown for two tubes in Figure 2C, whereby the growth rate was given by the slopes of the kymograph edges. Under the conditions used here (500 mM NaCl), extremities of capsid tubes grew at a rate of  $0.52 \pm 0.17 \text{ nm/s}$  in each direction (Figure 2D).

We observed that the fluorescence intensity along the tubes varied considerably between tubes in the field of view (Figure S3B, SI). On the basis of the narrow distribution of tube diameters seen in the negative staining EM images (Figure 3), we speculated that this variation resulted from the growth of multiple tubes bundled together or of multiwalled tubes<sup>28</sup> rather than from the growth of individual tubes with varying



**Figure 2.** Growth of fluorescent CA tubes on surfaces. (A) Negative staining EM image of CA tubes assembled from A14C/E45C:K158C-AF488 (76  $\mu\text{M}$ :4  $\mu\text{M}$ ). (B) Time-lapse TIRF images showing the growth of immobilized fluorescent tubes assembled from A14C/E45C:K158C-AF488 (76  $\mu\text{M}$ :4  $\mu\text{M}$ ) over 30 min. (C) Kymographs for two selected tubes highlighted in the last image in panel B. (D) Histogram of growth rates determined from the slopes of the edges in kymographs ( $N = 515$  tubes).



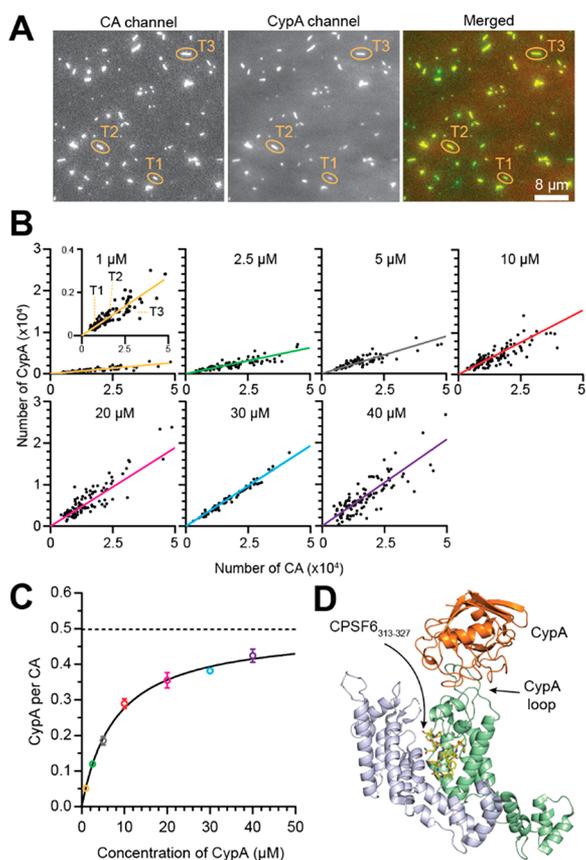
**Figure 3.** Growth of individual tubes in the presence of CypA. (A) Negative staining EM image of CA structures assembled from A14C/E45C:K158C-AF488 (76  $\mu\text{M}$ :4  $\mu\text{M}$ ) in the presence of CypA (10  $\mu\text{M}$ ). (B) Boxplots of tube diameters measured from EM images of four different assembly reactions of CA A14C/E45C:K158C-AF488 (76  $\mu\text{M}$ :4  $\mu\text{M}$ ) in the absence ( $N = 209$ ) and presence ( $N = 605$ ) of CypA, nested  $t$  test (two-tailed). (C) Histograms of the number of fluorophores per unit length (tubes and bundles) grown on the biosensor surface in the absence ( $N = 10\,941$ ) and presence of CypA ( $N = 49\,839$ ).

diameters. It has been shown that wild-type CA tube bundling can be minimized by addition of CypA, an 18 kDa globular protein that binds reversibly to the outside of CA tubes.<sup>27</sup> Assembly of tubes in solution from CA A14C/E45C and labeled CA K158C in the presence of substoichiometric amounts of CypA yielded primarily single tubes with a diameter of  $62.3 \pm 7.1$  nm (indistinguishable from tubes assembled in the absence of CypA with a diameter of  $63.6 \pm 7.6$  nm), as determined by negative staining electron microscopy (Figure 3A,B). Some of the tubes appeared to have closed ends. Short tubular or conical structures were also observed.

Next, we tested whether addition of CypA during CA tube growth on surfaces could suppress tube bundling. We grew tubes on surfaces in the absence and presence of CypA and identified fluorescent lines in the TIRF images using an automated image analysis algorithm (Figure S4, SI). Analysis of >10 000 line-shaped objects showed a linear relationship between the number of fluorophores versus the length for both conditions (Figure S5, SI), allowing us to represent the data as distributions of fluorophores per unit length. Assembly of CA A14C/E45C and labeled CA K158C in the presence of CypA yielded line-shaped objects with a narrow distribution centered at 223 fluorophores/ $\mu\text{m}$  (Figure 3C, right); we assign this linear density of label incorporation to that of single CA tubes grown on the sensor surface. While the majority of objects in this condition were single tubes, the asymmetry of the distribution with a shoulder at higher linear densities indicated that some tube bundles may still be present. In contrast, the distribution of fluorophores per unit length for elongated objects assembled in the absence of CypA was broad with a peak at 604 fluorophores/ $\mu\text{m}$  (Figure 3C, left), indicating that most objects assembled in the absence of CypA represent tube bundles with on average three tubes. Taken together our data suggest that CypA present during tube growth effectively

suppresses tube bundling, allowing us to prepare surfaces with predominantly single tubes. CypA dissociates rapidly from CA tubes after washout from the flow channel,<sup>22</sup> such that CypA used during assembly is no longer present during subsequent biosensor measurements. On the basis of the number of fluorophores per unit length measurement for single tubes and the packing of CA molecules in the hexameric lattice (Figure S6, SI), we estimated that approximately 1:53 CA molecules in the lattice were labeled with a fluorophore, similar to the labeling ratio determined biochemically (1:39, see Supporting Results and Figure S1, SI). The labeling ratio provided a calibration factor to determine the stoichiometry of analyte binding to capsid tubes in the biosensing experiments described below. Overall our experiments defined parameters for growing individual fluorescent tubes of uniform intensity on passivated surfaces as biorecognition elements, whereby the ability to measure the growth kinetics could also be exploited to test the effects of HIV-1 capsid assembly inhibitors.<sup>29</sup>

**Biosensor Assay To Measure CypA Equilibrium Binding Curves.** In the first application of our biosensor, we used equilibrium binding measurements to determine the dissociation constant ( $K_d$ ) and stoichiometry of the CypA–CA complex on CA tubes. CypA is an abundant host cell protein that binds to the CypA binding loop located on the N-terminal domain of CA (Figure 4D). Recruitment of multiple CypA molecules onto the outside of the HIV-1 capsid after host cell entry promotes HIV-1 infection,<sup>30</sup> but the precise binding mode of CypA to assembled CA lattices remains unclear. A solution containing CypA labeled at Cys52 with Alexa Fluor 647 was injected into the flow channel while the fluorescence signals of the cross-linked CA tubes and CypA were imaged by dual-color TIRF microscopy. CypA fluorescence appeared rapidly in the CypA channel at locations corresponding to immobilized tubes and reached a constant intensity upon reaching binding equilibrium (Figure 4A). The CypA solution was then washed out and the cycle was repeated for a range of CypA concentrations (1–40  $\mu\text{M}$ ), whereby we used the same flow channel to demonstrate the reusability of the biosensor interface for multiple measurements. Using automated image analysis we then extracted the number of CA and CypA molecules associated with each tube from the fluorescence intensities in the respective channels (Figure 4B). At any given concentration, the number of bound CypA molecules increased linearly with the number of CA molecules in a tube; i.e., longer tubes bound proportionally more CypA molecules (see example tubes T1, T2, and T3 highlighted in the merged image of Figure 4A and in the inset of Figure 4B). We then calculated the molar binding ratio at each concentration (see Figure 4B for details) to obtain an equilibrium binding curve (Figure 4C). Curve fitting with an equilibrium binding model yielded a  $K_d$  of 8.0  $\mu\text{M}$  and a stoichiometry of 0.5 CypA per CA at saturation; i.e., half of the CypA binding loops on the CA lattice can be occupied simultaneously, as predicted on the basis of structure and simulations.<sup>27</sup> The  $K_d$  determined here for the CypA–CA tube interaction was in the range of values for the complex of CypA with unassembled CA previously determined.<sup>4,31,32</sup> Our observations with CypA as an analyte demonstrate the application of the biosensor for accurate affinity measurements, whereby calibration of the response with the intensity of a single molecule also allowed counting of molecules and thus measurement of molar binding ratios. We have recently demonstrated the utility of this analysis by testing the

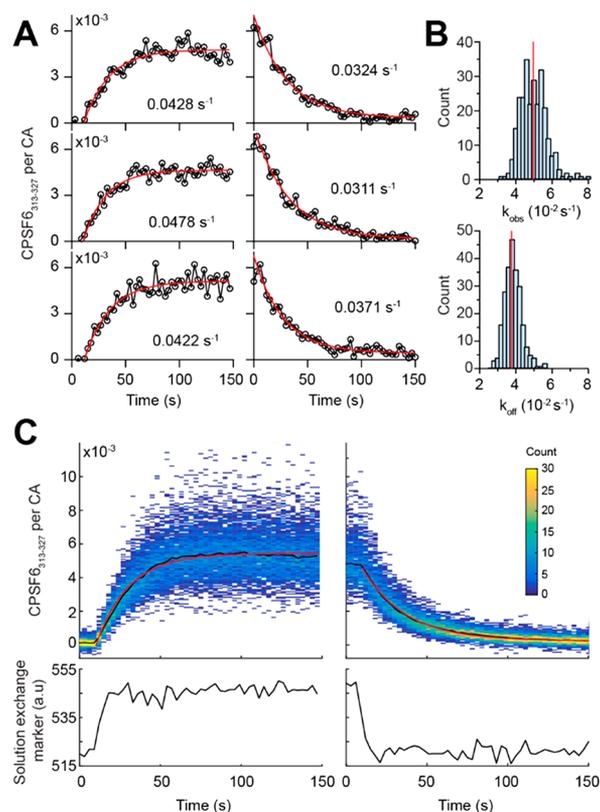


**Figure 4.** Affinity and stoichiometry of CypA binding to CA tubes. (A) TIRF images of CA A14C/E45C:K158C-AF488 tubes (left), CypA-AF647 (1  $\mu\text{M}$ ) (middle), and the overlay of both channels (right). (B) Scatter plots of the number of CypA molecules versus the number of CA molecules per tube after injection of CypA (1–40  $\mu\text{M}$ ); each symbol represents an individual tube. The CypA:CA ratio for each concentration was obtained from the gradient of the line of best fit (colored line). The inset shows a zoomed-in view of the scatter plot recorded at 1  $\mu\text{M}$  CypA-AF647, whereby the data points labeled T1, T2, and T3 correspond to the three tubes highlighted in panel A. (C) Equilibrium binding curve obtained by plotting the CypA:CA ratio as a function of CypA concentration. Error bars represent the mean  $\pm$  standard deviation of at least three fields of view on the sensor surface. The fit of an equilibrium binding model (black line) estimated a  $K_d$  of 8.0  $\mu\text{M}$  and a CypA:CA molar binding ratio at saturation of 0.5. (D) Structural model showing two neighboring CA molecules (blue and green) of a hexamer in complex with CypA (orange) and CPSF6<sub>313–327</sub> peptide (yellow stick model). Generated from PDB 1AK4,<sup>7</sup> 4U0A,<sup>10</sup> and 3H47.<sup>33</sup>

functionality of a proposed secondary CA binding site on CypA.<sup>22</sup>

**Biosensor Assay To Measure CPSF6 Peptide Binding and Dissociation Kinetics.** Next, we performed time-resolved biosensor measurements to determine the kinetics of biomolecular interactions on capsid tubes. As an example analyte, we used an Alexa Fluor 488-labeled peptide derived from CPSF6 (residues 313–327), a host cell protein that promotes nuclear import and integration targeting of the viral DNA via interactions with the CA lattice.<sup>34,35</sup> CPSF6<sub>313–327</sub> binds into a pocket formed between adjacent CA molecules in a hexamer (Figure 4D) with low affinity ( $K_d$  of 50–100  $\mu\text{M}$ ).<sup>9</sup> The analyte was injected into the flow channel at a concentration (250 nM) that was >100-fold below the  $K_d$ , i.e., conditions that should lead to less than 1% occupation of

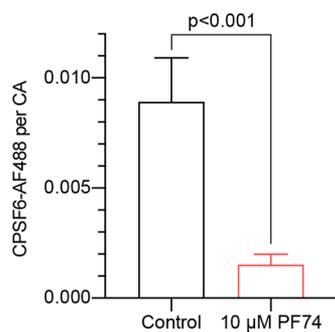
available binding sites. To perform kinetics measurements, we used time-lapse dual-color TIRF microscopy to monitor the appearance and subsequent disappearance of the CPSF6<sub>313–327</sub>-AF488 signal during analyte injection and subsequent washout in the flow channel (Figure S7, SI). Using the JIM Immobilized Microscopy Suite of programs (freely available from a GitHub repository, see Materials and Methods) for automated detection of CA tubes and extraction of background-corrected fluorescence signals, we then extracted CPSF6<sub>313–327</sub>-AF488 binding and dissociation traces for each CA tube in a field of view. Example single-tube traces are shown in Figure 5A and the heatmap of all traces is shown in Figure 5C. Kinetic rate constants for binding ( $k_{\text{obs}} = 4.96 \times 10^{-2} \text{ s}^{-1}$  at 250 nM) and dissociation ( $k_{\text{off}} = 3.77 \times 10^{-2} \text{ s}^{-1}$ ) could readily be obtained by curve fitting of individual traces (Figure 5A,B) or median traces (Figure 5C). The molar binding ratio at equilibrium reached a value of  $0.0049 \pm$



**Figure 5.** Binding and dissociation kinetics of CPSF6 peptide on CA tubes. (A) CPSF6<sub>313–327</sub>-AF488 binding (left) and dissociation (right) traces measured on different capsid tubes during CPSF6<sub>313–327</sub>-AF488 injection (250 nM) and washout, respectively. The rate constants ( $k_{\text{obs}}$  for binding and  $k_{\text{off}}$  for dissociation traces) were determined from least-squared exponential fitting (red line) of the fluorescence traces. (B) Histograms of values obtained for  $k_{\text{obs}}$  (top) from fitting individual binding traces ( $N = 272$  tubes) and for  $k_{\text{off}}$  from fitting individual dissociation traces ( $N = 238$  tubes). The red lines indicate values from the fitting of median traces in panel A. (C) Heatmaps (top) showing the CPSF6<sub>313–327</sub>-CA ratio for all tubes in the field of view during CPSF6<sub>313–327</sub>-AF488 injection (250 nM, left) and washout (right). The median CPSF6<sub>313–327</sub>-AF488 traces (black line) were fitted with exponential functions (red line) to give rate constants of  $k_{\text{obs}} = 4.96 \times 10^{-2} \text{ s}^{-1}$  and  $k_{\text{off}} = 3.77 \times 10^{-2} \text{ s}^{-1}$ , respectively. The signal of a marker for solution exchange in the flow channel is shown in the plots at the bottom.

0.0001 CPSF6<sub>313–327</sub> per CA (i.e., 0.5% occupation of binding sites), as expected for the low analyte concentration, but the signal was readily detectable above noise at levels corresponding to 0.1% occupation of binding sites [Figures S5A and S7 (SI)], suggesting that binding should be detectable at analyte concentrations that are up to 3 orders of magnitude below the  $K_d$  of the interaction. Weak interactors with a  $K_d$  of one to a few hundred micromolar (such as CPSF6<sub>313–327</sub>) are presumably close to the upper limit of the affinity range for analytes that can be detected with this biosensor before the signal becomes no longer detectable against background fluorescence from analyte in solution.

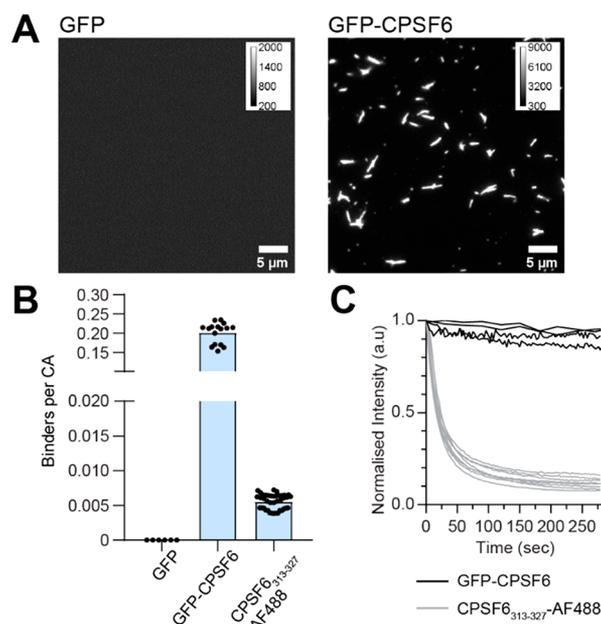
**Binding Competition between CPSF6 Peptide and PF74.** The antiviral drug PF74 targets the same binding pocket on the CA hexamer as CPSF6<sub>313–327</sub> and inhibits HIV-1 infection soon after release of the viral capsid into the cytoplasm.<sup>9,36,37</sup> PF74 is thought to act via multiple mechanisms; e.g., it may prevent functional interactions of host proteins (such as CPSF6) with the HIV-1 capsid. Addition of PF74 to the biosensor assay significantly decreased the binding signal of CPSF6<sub>313–327</sub>-AF488 on CA tubes [Figures 6 and S8 (SI)] as expected for the binding



**Figure 6.** PF74 inhibits CPSF6<sub>313–327</sub> binding. Bar graph of CPSF6<sub>313–327</sub>-AF488 molecules per CA bound to CA tubes in the absence ( $N = 35$ ) and presence ( $N = 34$ ) of 10  $\mu$ M PF74. Error bars represent the standard deviation, using the unpaired two-tailed Welch's  $t$  test.

competition between these two molecules for the same site on the CA lattice. This experiment highlights the potential applications of the CA tube biosensor for measuring binding competition to the CA lattice and testing of competitive inhibitors of capsid-binding host cell proteins that are utilized by HIV-1 to facilitate infection.

**Binding Analysis of CPSF6 Produced by Cell-Free Protein Expression.** Finally, we tested the compatibility of the biosensor with GFP-fusion proteins produced by cell-free expression, a rapid method for producing recombinant proteins in microtiter plates for screening protein–protein interactions.<sup>24,38</sup> Expression of full-length CPSF6 fused at its N-terminus to GFP (GFP-CPSF6) in *Leishmania* extract yielded a mixture of different oligomeric states (Figure S9, SI), as previously observed for N-terminally tagged CPSF6<sub>1–358</sub> expressed in mammalian cells.<sup>39</sup> In contrast, expression of GFP as a control protein yielded monomers (Figure S9, SI). We then injected cell-free expressed proteins without further purification (adjusted to a concentration of 370 nM) into the flow channel of the biosensor to detect the equilibrium binding level of the proteins on CA tubes. As expected, GFP did not bind to the sensor interface (Figure 7A,B). GFP-CPSF6 bound



**Figure 7.** Binding analysis of proteins produced by cell-free expression. (A) TIRF images of the analyte channel after injection of GFP (left) and GFP-CPSF6 (right). (B) Bar graph of the molar binding ratio between analyte to CA. Each symbol represents the median value from a field of view taken from at least two different flow channels. (C) Dissociation traces of GFP-CPSF6 and CPSF6<sub>313–327</sub>-AF488 during washout. Each curve represents a separate experiment.

strongly to the tubes (Figure 7A) and reached a level of  $0.20 \pm 0.03$  molecules per CA (Figure 7B), which decayed slowly after washout (Figure 7C), while the signal of CPSF6<sub>313–327</sub>-AF488 reached a 30-fold lower level and decayed rapidly (Figure 7B,C). These observations are consistent with a strengthening of the CPSF6–capsid interaction through avidity and with oligomerization playing an important role in recognizing viral capsids, as suggested before.<sup>39</sup> Further experiments are needed to identify the physiologically relevant oligomeric species and dissect their effects on the functions of CPSF6 in the viral replication cycle.

## CONCLUSIONS

Our TIRF-imaging-based biosensor is ideal for time-resolved and quantitative interaction measurements between capsid-binding molecules and HIV-1 CA tubes to obtain kinetic rate constants, binding affinity, and stoichiometry. The key advantages of this system are its stability and surface reusability, which allows robust detection of analyte binding at levels corresponding to single molecules per viral capsid (i.e., one analyte per 1500 CA molecules). The appearance of the capsid tubes as lines in the fluorescence image facilitates detection and extraction of traces using automated image analysis. Tubular CA lattices are commonly used in binding studies as surrogates for the capsid<sup>16,18,40,41</sup> but they lack CA pentamers and the variable curvature of the native conical capsid. Combining our biosensor as a tool for routine measurements with more specialized approaches using virus-like particles<sup>32</sup> should overcome these limitations.

The ability to monitor binding dynamics of different species labeled with distinct fluorophores at the level of single tubes with high sensitivity and temporal resolution opens the door to

resolving binding cooperativity and competition, similar to TIRF-based measurements of other linear biopolymers.<sup>42–45</sup> The compatibility of the biosensor with complex samples and low reagent usage could facilitate analysis of proteins in mammalian cell lysates that are otherwise difficult to produce (such as CPSF6<sup>39</sup> and TRIM5 $\alpha$ <sup>41,46</sup>) and rapid screening of potential new interactors of the HIV-1 capsid produced by cell-free expression. Proof-of-principle measurements demonstrated the utility of the HIV-1 capsid biosensor for testing binding modes of host proteins involved in promoting HIV-1 infection, suggesting a role for oligomerization in CPSF6 binding. The underlying design can conceptually be extended to other viruses<sup>47–50</sup> for discovery and characterization of proteins, small molecules, and drugs that interact with viral capsids to facilitate or inhibit gene delivery and viral replication.

## ■ ASSOCIATED CONTENT

### ■ Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsami.9b08521.

Supporting Materials and Methods and Supporting Results sections and Figures S1–S9 (SDS–PAGE analysis of CA K158C fluorescence labeling kinetics and assembly efficiency; negative staining EM of CA tubes with and without labeled CA K158C; TIRF images of CA tubes grown on surfaces with and without antibody; output of analysis software developed for automated detection and masking of capsid tubes in fluorescence images; heatmaps of the number of fluorophores as a function of length for elongated structures grown on the sensor surface in the absence and presence of CypA; schematic of CA tube geometry; TIRF images of CPSF6<sub>313–327</sub>-AF488 binding and dissociation; competition of CPSF6<sub>313–327</sub>-AF488 with PF74; single-molecule spectroscopy of proteins produced by cell-free expression using *Leishmania* extract) (PDF)

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### Author Contributions

D.L. provided protein production/labeling/assembly, assay development, the TIRFM binding assay with CypA and CPSF6, and data analysis and helped write the original draft. J.W. furnished software and data analysis and reviewed and edited the manuscript. W.P. investigated the TIRFM binding assay with CypA, performed data analysis, and reviewed and edited the manuscript. V.S. supervised the experiments and reviewed and edited the manuscript. S.T. supervised the experiments and reviewed and edited the manuscript. D.J. supervised the experiments and helped write the original draft. T.B. conceptualized and supervised the experiments and wrote the original draft.

### Notes

The authors declare no competing financial interest.

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